

## **APPLIED FSI TECHNIQUE TO INITIAL INSIGHT INTO THE RESULT OF EXERCISE ON THE SEMILUNAR VALVE SW**

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**Abstract:** The left ventricle stroke work may be a function of the work done by the heart ventricle throughout the ejection of blood throughout per oscillation. The aim of this investigation was to propose a model to numerically evaluate the stroke work for a healthy subject by employing a FSI simulation throughout exercise protocol. Semilunar valve dimensions were calculated mistreatment Associate in nursing imaging technique of diagnostic procedure. Associate in Nursing FSI simulation was performed mistreatment Associate in nursing ALE mesh. Boundary conditions were outlined by pressure masses on cavum and arterial blood vessel sides. Stroke work was foretold to extend to 121% from sixty mm. to a hundred twenty-five mm, and it didn't increase abundantly on top of a hundred twenty-five mm. Supported derived regression equations of our FSI results for stroke work and comparison of them with clinical ones, numerically-predicted stroke work values are in smart agreements with printed clinical knowledge. The slope of stroke work changes to mean blood pressure, whereas exercise protocol, is 168.08 milliliter that is twelve.2% below the common slope of clinical knowledge. The coordinate axis intercept of stroke work changes to mean blood pressure, whereas exercise protocol, is -11186 mmHg.ml that is V-J Day below the common coordinate axis intercept of clinical knowledge. Our results for the particular patient show that numerical ways are often projected to predict smart estimates of patient-specific stroke work completely different heart rates.

**Keywords:** *Fluid Structure Interaction (FSI), absolute Lagrangian Eulerian (ALE), Stroke Work (SW), Left cavity stroke-work index (LVSWI) versus left cavity end-diastolic pressure (LVEDP).*

**INTRODUCTION:** Measurement of stroke work may be a crucial think about understanding the development of heart issues and sequent clinical diagnosing. As an example, the stroke work index may be a reliable criterion of left ventricle performance which needs associate degree invasive procedure and has been typically measured and used within the settings of medical aid units and operation rooms. Whereas invasive ways are wont to measure stroke work, such techniques square measure valuable and embrace risks to patients. Procedure procedures, however, have the potential to determine stroke work, however, bypassing such limitations. Invasive and value intensive techniques are used to date. For example, Loeb et al. assessed the left cavity to operate once acute myocardial infarction victimization stroke volume calculation. They aforesought left cavity stroke-work index versus left cavity end-diastolic pressure. Linhart investigated pacing-induced alterations in stroke volume within the appraisal of heart muscle operate. They performed right chamber pacing in sixteen subjects whereas right and left heart catheterizations. They all over once pacing cavity function curves were performed relating left cavity stroke work to LVEDP, traditional patients incontestable a steep curve. Hamosh and Cohn studied acute MI with measurement left ventricular stroke volume. Hamosh and Cohn in forty healthy patients estimated the accuracy of stroke volume via reservoir pressure idea and three-part. Also, thanks to the actual fact that invasive experiments might be risky for a human subject, there are some studies on animals; although no information relating to stroke work was found in a number of them, it will be derived from their hemodynamic results. Simultaneous simulations of Fluid-Structure Interaction (FSI) have the potential for non-invasive prediction of stroke work. Recently, FSI has been used to analyze heart and heart valve mechanics. Studies embrace the use of a two-dimensional model to judge the stroke volume and flow rate for a healthy subject. That was done by coupling the FSI simulation with associate degree echo-Doppler methodology at rest and while exercise. Careful attention was taken into consideration to validate the simulation against viscous operate measures that may be dependably computed by victimization clinical protocols, with variable heart rates. Moreover, it had been attainable to predict the impact of pulse rate increment while sweating on blood hemodynamic through the semilunar valve and strains and stresses toughened by the valve leaflets. Developing such models to alter stroke work would doubtless be of clinical value as a result of their imagined to perform it a lot of promptly. However, so far FSI and clinical measurements haven't been articulate to predict a Patient's stroke work. Impact of pulse rate changes on stroke work of the patient haven't been analyzed either. Heart rate would be a big parameter concerning as a result of it brings about large variations in stroke work. The aim of this analysis was to assess the influence of exercise on stroke work on totally different heart rates from rest to exercise. Victimization FSI model and our two-dimensional semilunar valve pure mathematics, we have a tendency to appraise stroke work during exercise. The key valves of dimensions and boundary conditions for

our study were noninheritable from one volunteer, sanctioning associate degree initial assessment of the relevance of the model for personalized health care.

**Materials and ways Overview:** A healthy human male adult, thirty-three years previous (80 kilos, 175 cm, BMI: 26.1), participated in this study. His healthy vas operate was confirmed by clinical protocols. The consent was obtained. The workflow of the study is provided in Figure one.

**Numerical approach:** Systolic and pulse pressures were recorded throughout the check via a limb pressure cuff (Figure 2). Victimization echo-cardiography, the aortic valve pure mathematics (Figure 3) and its dimensions were obtained (Table 1). The pc motor-assisted style (CAD) model of the semilunar valve geometry was created with Solid works package supported the clinically measured data. The leaflet mechanical properties were thought of as Homogenous, identical with the linear stress-strain relationship. Blood was likely to be Newtonian associate degreed an incompressible fluid. All material properties square measure given in Table two.

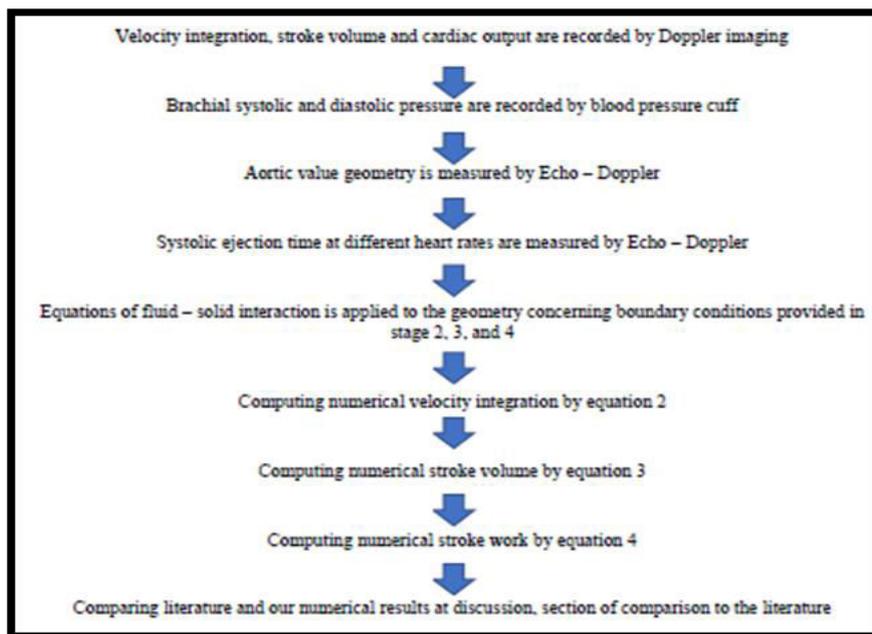


Figure 1: Flow of Work Model

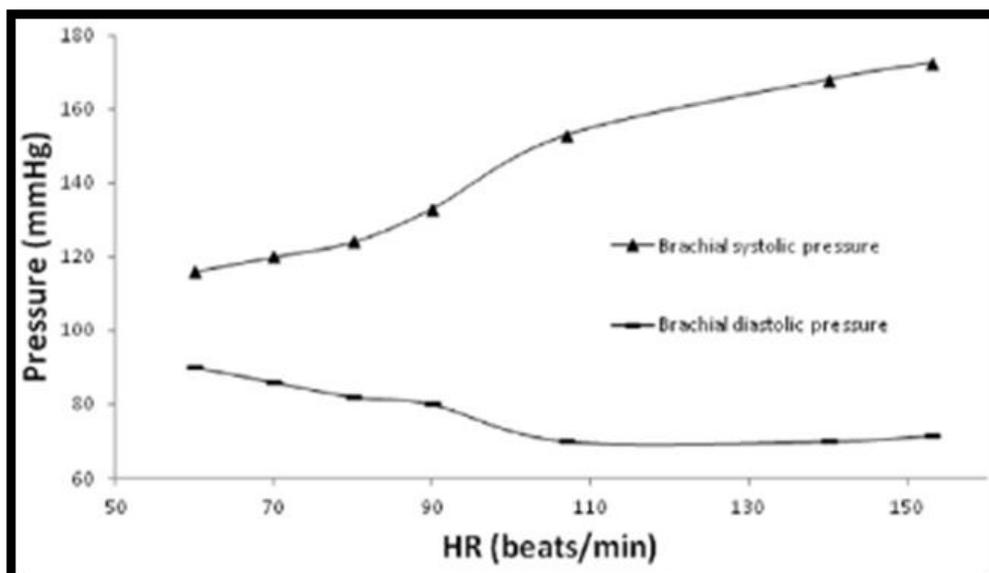
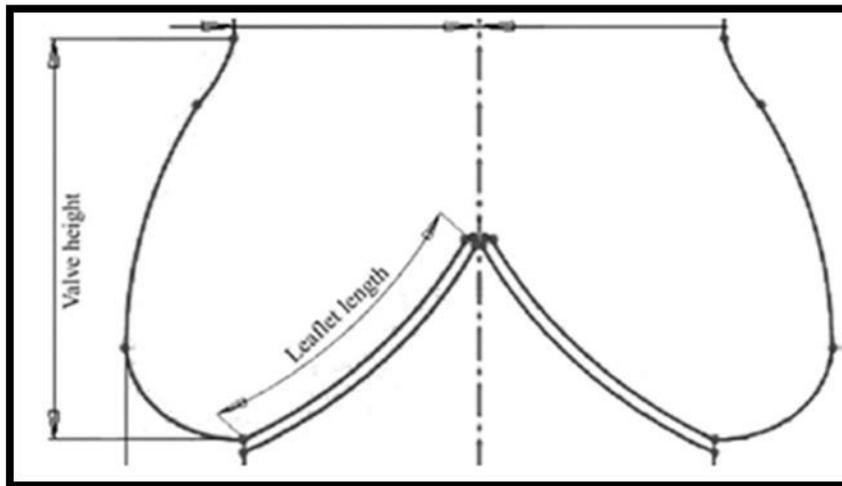


Figure 2: Systolic & Diastolic Pressures.



**Figure 3: 2-D aortic valve geometry**

The CAD model then discretized and imported into the finite element analysis package, comsol Multi-physics. The fluid and structure governing equations were applied and also the material geometries were introduced. Pressure boundary condition was used at the flow (the bodily cavity side) and outflow (the arterial blood vessel side) boundaries for the mechanic's module (Figure 3). The employment of a moving beer mesh enabled the deformation of the fluid mesh to be half-track while not the necessity for re-meshing. The second order Lagrangian components were utilized to outline the mesh. The model is capable to unravel time-dependent FSI model. The model then valid to confirm its independence from mesh resolutions.

**Analysis of fluid dynamics:** For FSI simulations, the mean rate numerically was obtained at every time step of the ejection amount. Comparison of measurements of rate integration, flow and stroke volume enabled quantitative validation of the FSI model. Knowing the speed integration and arterial blood vessel space, one will calculate the stock volume:

$$\text{Stroke volume} = \text{Velocity integration} \times \text{arterial blood vessel space}$$

The total left bodily cavity stroke work (SW) is calculated by the product of left bodily cavity pressure throughout ejection and also the ejected the volume of blood integrated over the ejection interval (Figure 3).

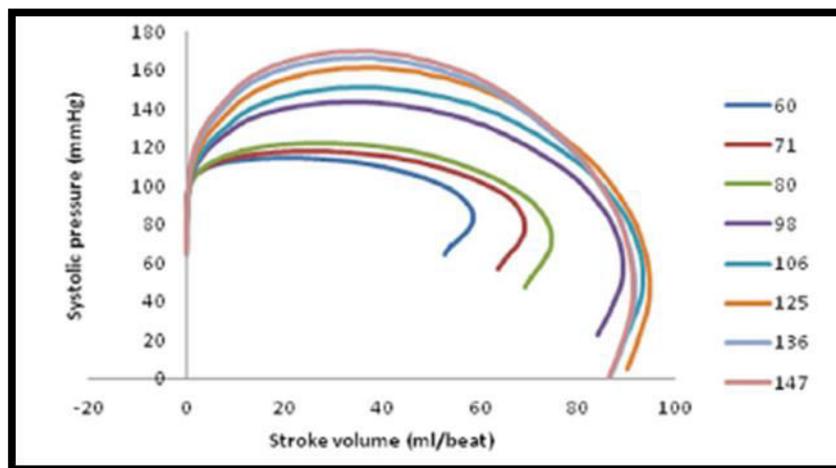
**Results:** Systolic pressure changes to stroke volume Figure four provides blood pressure changes to stroke volume at different heart rates. Overall, in terms of ascending and downward-sloping heart rates, all the curves follow an equivalent trend. However, as the rate increases, the curve size becomes larger. It may be ascertained that at the end of every curve, a stroke volume decreases. This reduction in stroke volume will indicate the blood back flowing towards heart ventricle. As seen in Figure four, the changes from the rate of sixty to eighty gait square measures abundant lower than those between the rate of ninety-eight to 147 gaits and also the next ones. Figure five provides the stroke work values throughout the ejection amount while increasing the centre rate. A multinomial equation with a high accuracy was fitted to the calculated knowledge. The stroke works through exercise protocol enlarged by 121% from sixty to one hundred twenty-five gaits, and it failed to increase abundant higher than one hundred twenty-five gaits. In a very healthy subject, at higher heart rates the filling time of the heart ventricle throughout pulsation will decrease that brings down the preload and as a result of this, the stroke volume won't show acceptable inculcation. This is often as a result of-of the very fact that the stroke volume doesn't increase significantly at the heart rate over one hundred twenty-five gaits. Stroke volume changes were followed by a bigger increment when the heart of eighty (Figure 4).

#### **Discussion Study findings**

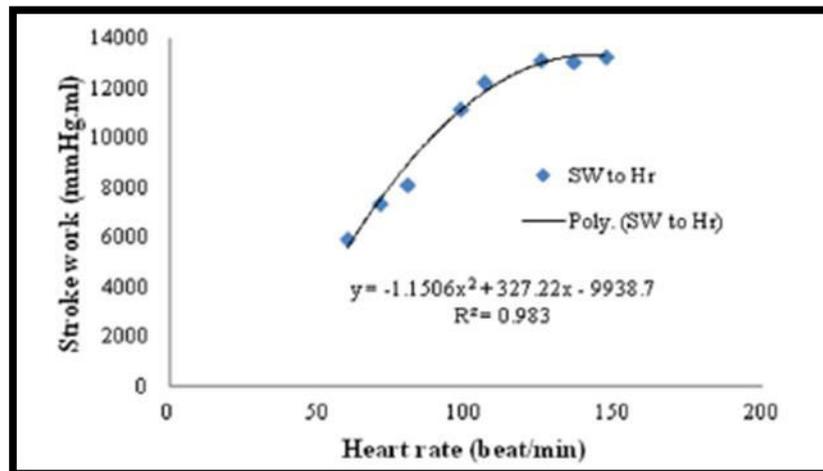
The study has investigated the initial use of a fluid-structure interaction model to calculate the stroke work done by the heart ventricle by scheming the pressures and blood flow volume through the arterial blood vessel valve. The hemodynamic knowledge was nonheritable from a healthy subject whereas exercising. Echo-Doppler-derived knowledge provided essential data for simulation together with semilunar valve pure mathematics and pressure boundary conditions. To the authors' information, this is able to be the primary time that exercise protocol measurements and FSI technique are combined along to alter numerical estimations of stroke work. All the curves of blood pressure changes to stroke volume at every heart

Follow an equivalent pattern at totally different heart rates in terms of ascending and downward-sloping orders (Figure 4). To any or all appearances, stroke volume variations when rate eighty, is followed by AN abrupt increase.

The FSI model foretold stroke run through an exercise protocol to increase by 121% from sixty to one hundred twenty-five gaits, so it failed to increase much higher than one hundred twenty-five gaits. Our investigation provides initial insight as for the practicableness of gaining a range of conditions (e.g. changes thanks to exercising). The pertinence of the modelling and its privileges admire low machine time and fewer pricey as compared to presently available clinical approaches; create it usable to estimate the stroke work in patients. in addition as aforementioned edges, our mathematical model has the potential to analyses totally different arterial blood vessel geometries. Also, this model let patients predict some things that aren't attainable to clinically live. To be additional actual, supported the very fact that the topic is soul applying such numerical model let physicians understand and investigate probable conditions wherever patients might face within the future or on totally different circumstances. Etiology of pathological states would be what is more assessable sin they may result in form and kind (geometry) undulation and amount of blood pressure (boundary conditions). On high of that, the overwhelming majority of clinical techniques and analysis aren't mechanical-based. Taking into the thought that the character of heart valve functions is usually mechanical-based, our discipline apparently steps toward to analyze the heart performance because it may be a mechanical pump to an excellent extent.



**Figure 4:** Systolic pressure changes to stroke volume at different heart rates.

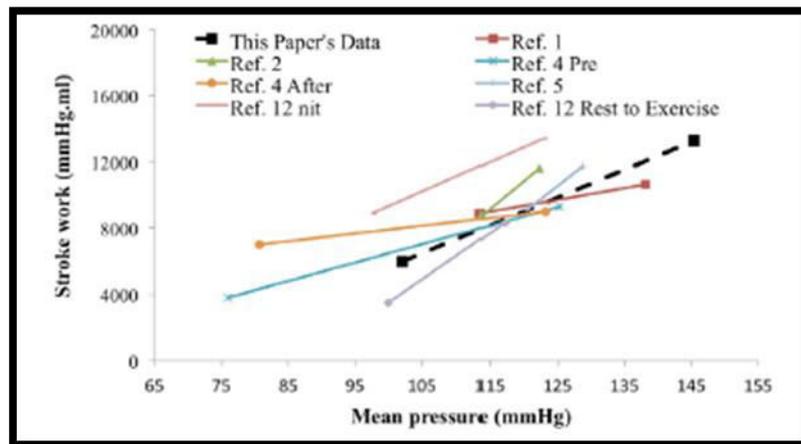


**Figure 5:** Stroke work changes to heart rate.

**Application and Responsibleness:** Catheterization-Thermo dilution is understood because of the golden methodology for measuring internal organ perform this is often, however, AN invasive technique. This has been established such ways square measure related to potential perils together with cardiopathy, death, and even heart disease. The FSI modelling can give clinical team data that are clinically compatible with Catheterization-Thermo dilution and supply such knowledge earlier and in a very safer approach than ancient strategies. Non-invasive measurement of the hemodynamic parameters and knowing the traditional values for these parameters, the hemodynamic standing of every patient can be delineated as p.c changes from the norm. This may result in

numerical modelling of the hemodynamic standing, and clinicians could be able to additionally accurately react to the individual wants of the patient with acceptable treatment. Moreover, numerical simulations square measure capable to exactly estimate internal organ hemodynamic. This is often largely due to the very fact that it doesn't cope with inter- and intra-observer validity variables that square measure chiefly the argument for playing graphical record. This kind of unevenness is contingent upon personal experience and also the image capture ability of the user. Therefore, the elemental matter is to prove the believability of modelling strategies for internal organ evaluations. Moreover, clinical experiments performed on animal subjects. Amezcua et al. incontestable to avoid any risks for human subjects will glorify the deserves of numerical approaches.

**Comparison:** Figure six performs stroke work changes to mean blood pressure (for the exercise protocol). Because it may be ascertained, the slope of the results.



**Figure 6:** FSI and clinical stroke work changes to mean

The average slope of clinical knowledge is 191.42 mmHg·ml/ml. The rumored reported by this paper and square measure at intervals the reported clinical knowledge varied from 46.56 to 335.05 ml [1, 2, 4, 5, 12]. The results of this paper square measure at intervals twelve.2% with the literature rumored knowledge. The variations may well be thanks to weight, sex, age, and race of patients. It can be all over that the rumored knowledge from the numerical model in this paper is in an appropriate varying of rumored clinical knowledge.

**Limitations & future trends:** The limitations of this numerical study and future suggestions square measure listed as following:

- ✓ Exploitation two-dimensional instead of three-dimensional pure mathematics.
- ✓ Applying linear, undiversified and identical options for
- ✓ Simplification of arterial blood vessel valve's mechanical properties.
- ✓ A mechanical properties square measure supported generalized data, and aren't specific to the patient.
- ✓ Considering blood as a Newtonian and incompressible fluid.
- ✓ Despite model limitations, we have a tendency to consummate an appropriate consistency with the final literature.

Undoubtedly, a three-dimensional model could end in additional precise predictions; but, it might even be rising the process time (that is a smaller amount than quarter-hour for the two-dimensional model). This should hold shortcomings for clinical applications.

**CONCLUSION:** We have given a two-dimensional fluid-structure interaction simulation of the semilunar valve having the power to predict stroke work from rest to exercise stage. Derived regression for stroke work changes versus mean blood pressure showed the averagely V-day distinction between numerical and clinical knowledge. Thus, this model provides initial insights as the potential for predicting stroke work for a selected individual at intervals a 15-minute time interval that matches with clinical knowledge.

## REFERENCES

1. Carrick-Ranson G, Doughty RN, Whalley GA, Walsh HJ, Gamble GD, et al. (2012) the larger exercise stroke volume in endurance-trained men does not result from increased left ventricular early or late inflow or tissue velocities. *Acta Physiologica* 205: 520-531.
2. Bouchard MJ, Denault A, Couture P (2004) Poor correlation between hemodynamic and echocardiographic indexes of left ventricular performance in the operating room and intensive care unit. *Crit Care Med* 32: 644-648.

3. Gunzinger R, Heimisch W, Augustin N (2005) Diastolic unloading and improved LV pump efficiency early after repair of the insufficient mitral valve. *Thorac Cardiovasc Surg* 53: 9-15.
4. Baba HA, Wohlschlaeger J, Stubbe HD (2004) Heat shock protein 72 and apoptosis indicate cardiac decompensation during early multiple organ failure in sheep. *Intensive Care Med* 30:1405-1413.
5. Lavdaniti M (2008) Invasive and non-invasive methods for cardiac output measurement. *Int J Caring Sci* 1:112-117.
6. Hofer CK, Ganter MT, Zollinger A (2007) What technique should I use to measure cardiac output? *Curr Opin Crit Care* 13: 308-317.
7. Engoren M, Barbee D (2005) Comparison of cardiac output determined by bioimpedance, thermodilution, and the Fick method. *Am J Crit Care* 14: 40-45.
8. Loeb HS, Rahimtoola SH, Rosen KM, Sinno MZ, Chuquimia R, et al. (1973) Assessment of ventricular function after acute myocardial infarction by plasma volume expansion. *Circulation* 47: 720-728.
9. Linhart JW (1971) Pacing-induced changes in stroke volume in the evaluation of myocardial function. *Circulation* 43: 253-261.
10. Hamosh P, Cohn JN (1971) Left ventricular function in acute myocardial infarction. *J Clin Investigation* 50: 523
11. Kamoi S, Squire D, Revie JA, Chase JG (2014) Accuracy of stroke volume estimation via reservoir pressure concept and three element windkessel model.
12. Amezcua JL, Palmer RMJ, Souza BD, Moncada S (1989) Nitric oxide synthesized from L-arginine regulates vascular tone in the coronary circulation of the rabbit. *British J Pharmacol* 97: 1119-1124.
13. Baydoun AR, Woodward B (1991) Effects of bradykinin in the rat isolated perfused heart: Role of kinin receptors and endothelium-derived relaxing factor. *British J Pharmacol* 103: 1829-1833.
14. Brown IP, Thompson CI, Belloni FL (1993) Role of nitric oxide in hypoxic coronary vasodilatation in isolated perfused guinea pig heart. *American J Physiol* 264: H821-H821.
15. Lamontagne D, Pohl U, Busse R (1991) N G-nitro-l-arginine antagonizes endothelium-dependent dilator responses by inhibiting endothelium-derived relaxing factor release in the isolated rabbit heart. *Pflügers Archiv* 418: 266-270.
16. Park KH, Rubin LE, Gross SS, Levi R (1992) Nitric oxide is a mediator of hypoxic coronary vasodilatation. Relation to adenosine and cyclooxygenase-derived metabolites. *Circulation Res* 71: 992-1001.
17. Smith RE, Palmer RM, Bucknall CA, Moncada S (1992) Role of nitric oxide synthesis in the regulation of coronary vascular tone in the isolated perfused rabbit heart. *Cardiovascular Res* 26: 508-512.
18. Ueeda M, Silvia, SK, Olsson RA (1992) Nitric oxide modulates coronary autoregulation in the guinea pig. *Circulation Res* 70: 1296-1303.
19. Al-Atabi M, Espino DM, Hukins DWL (2010) Computer and experimental modelling of blood flow through the mitral valve of the heart. *J Biomech SciEng* 5: 78-84
20. De Hart J, Peters GW, Schreurs PJ, Baaijens FP (2000) A two-dimensional fluid-structure interaction model of the aortic valve. *J Biomech* 33: 1079-1088.
21. De Hart J, Peters GW, Schreurs PJ, Baaijens FP (2003a) A three-dimensional computational analysis of fluid-structure interaction in the aortic valve. *J Biomech* 36:103-112.
22. De Hart J, Baaijens FP, Peters GW, Schreurs PJ (2003b) A computational fluid-structure interaction analysis of a fiber-reinforced stentless aortic valve. *J Biomech* 36: 699-712.
23. Espino DM, Shepherd DET, Hukins DWL (2012) A simple method for contact modelling in an arbitrary frame of reference within multiphysics software. *JMech* 29: N9 - N14
24. Espino DM, Shepherd DET, Hukins DWL (2013) Development of a transient large strain contact method for biological heart valve simulations. *Comput Methods Biomech Biomed Engin* 16: 413-424
25. Espino DM, Shepherd DET, Hukins DWL (2014) Evaluation of a transient, simultaneous, Arbitrary Lagrange Euler based multi-physics method for simulating the mitral heart valve. *Comput Methods Biomech Biomed Engin* 17: 450-458.
26. Stijnen JMA, De Hart J, Bovendeerd PHM, Van De Vosse FN (2004) Evaluation of a fictitious domain method for predicting dynamic response of mechanical heart valves. *J Fluids Struct* 19: 835-850.